RESEARCH





The Preventiometer - reliability of a cardiovascular multi-device measurement platform and its measurement agreement with a cohort study

Martin Junge^{1,2†}, Markus Krüger^{1,3*†}, Dietlind L. Wahner-Roedler⁴, Brent A. Bauer⁴, Marcus Dörr^{5,6}, Martin Bahls^{5,6}, Jean-François Chenot⁷, Reiner Biffar⁸ and Carsten O. Schmidt¹

Abstract

Background Multimedia multi-device measurement platforms may make the assessment of prevention-related medical variables with a focus on cardiovascular outcomes more attractive and time-efficient. The aim of the studies was to evaluate the reliability (Study 1) and the measurement agreement with a cohort study (Study 2) of selected measures of such a device, the Preventiometer.

Methods In Study 1 (N=75), we conducted repeated measurements in two Preventiometers for four examinations (blood pressure measurement, pulse oximetry, body fat measurement, and spirometry) to analyze their agreement and derive (retest-)reliability estimates. In Study 2 (N=150), we compared somatometry, blood pressure, pulse oximetry, body fat, and spirometry measurements in the Preventiometer with corresponding measurements used in the population-based Study of Health in Pomerania (SHIP) to evaluate measurement agreement.

Results Intraclass correlations coefficients (ICCs) ranged from .84 to .99 for all examinations in Study 1. Whereas bias was not an issue for most examinations in Study 2, limits of agreement for most examinations were very large compared to results of similar method comparison studies.

Conclusion We observed a high retest-reliability of the assessed clinical examinations in the Preventiometer. Some disagreements between Preventiometer and SHIP examinations can be attributed to procedural differences in the examinations. Methodological and technical improvements are recommended before using the Preventiometer in population-based research.

Keywords Method-comparison studies, Agreement, Reliability, Validity, Measurement, Bland-Altman Plots

[†]Martin Junge and Markus Krüger contributed equally to this work.

*Correspondence: Markus Krüger markuskr@uni-greifswald.de Full list of author information is available at the end of the article



© The Author(s) 2023. **Open Access** This article is licensed under a Creative Commons Attribution 4.0 International License, which permits use, sharing, adaptation, distribution and reproduction in any medium or format, as long as you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons licence, and indicate if changes were made. The images or other third party material in this article are included in the article's Creative Commons licence, unless indicated otherwise in a credit line to the material. If material is not included in the article's Creative Commons licence and your intended use is not permitted by statutory regulation or exceeds the permitted use, you will need to obtain permission directly from the copyright holder. To view a copy of this licence, visit http://creativecommons.org/licenses/by/4.0/. The Creative Commons Public Domain Dedication waiver (http://creativecommons.org/publicdomain/zero/1.0/) applies to the data made available in this article, unless otherwise stated in a credit line to the data.

Introduction

Over the last 50 years, the number and complexity of epidemiologic studies has grown and demands for participants has risen [1]. However, willingness to volunteer for scientific activities has declined, which is reflected by decreasing response rates [1-3]. Therefore, an initial refusal to participate in a study may not be interpreted as a general refusal of taking part in the study itself. Rather, constraints on participants' time and availability might make study demands appear too high. Therefore, making clinical examinations more efficient and attractive, using multimedia options, and making such offers closer to the participants' place of residence in a digital form or mobile platform might improve participation rates.

Digital solutions are already in use for surveybased research and are also increasingly applied to patient-reported outcome measures (PROMs). Beyond self-reported measures, wearables and smartphone applications are promising candidates that may also facilitate mobile measurement of medical variables [4, 5]. Another approach is taken by the Preventiometer (Fig. 1) [5, 6]. It is an interactive multi-device platform designed to assess prevention-related medical variables such as blood pressure, body fat, and pulse oximetry. During examinations, the participant takes place in a padded seat and looks at the inner side of a dome where videos are projected to (see Fig. 1). These videos contain instructions and background information on the examinations. The procedure can be controlled by the participant by pressing two buttons integrated into the armrest of the seat. The entire examination is accompanied by a study nurse who operates the control computer of the Preventiometer and monitors the measurement processes. The Preventiometer can be implemented in a mobile platform (e.g. a bus or van) to enable examinations closer to the participants place of residence. While the virtual assistant may contribute to a higher degree of standardization, the uncommon examination environment might also induce excitement, thereby impacting clinical measurements.

Acceptance of the Preventiometer by participants was previously assessed in a wellness context at Mayo clinics [7, 8]. Participants agreed or strongly agreed that it was both comfortable and engaging. In our current project *Prävention für Arbeitnehmer zur Reduktion von Krankheitstagen durch Motivation und Verhaltensänderung* ([preventive healthcare for workers with the aim to reduce absenteeism by motivation and behavior] PAKt-MV) [9] we evaluated the accuracy of the central measurement device as related results were not available from other studies.

In Study 1, we estimated the reliability by measuring participants twice within a Preventiometer and assessed the agreement between the repeated measurements. In Study 2, we estimated the measurement agreement of the Preventiometer with results of similar variables as obtained in the examination center of a population based cohort study, the Study of Health in Pomerania (SHIP) [10-12]. In both studies, only those examinations and variables of the Preventiometer that had a comparable examination in SHIP were included.

Study 1: agreement of repeated measurements within Preventiometers (Reliability)

The goal of Study 1 was to estimate the reliability of Preventiometer. Two Preventiometers at different locations in different environments were used in this study. One was on a mobile platform placed in a bus and the other one was stationary in a room of the local hospital. A stationary Preventiometer was used because only one bus was available. Participants were tested twice (repeated measure) with one of the Preventiometers. For efficiency and comparability between Study 1 and Study 2 we



Fig. 1 The mobile Preventiometer installed in a bus (Preventiometer 1)

selected only measures that were available for the Preventiometer and SHIP for Study 1.

Materials and methods

Study sample

A convenience sample of 22 males and 53 females with a mean age of 41.7 years (SD=13.3) in the range from 18 to 71 years participated. All participants were recruited among employees of the University Medicine of Greifswald and their families or acquaintances. All participants gave written informed consent. The Ethics Committee of the University Medicine Greifswald approved the study protocol.

Preventiometer

Two Preventiometers were used for the reliability assessment. The first Preventiometer was installed in an articulated bus (Mercedes-Benz Citaro G, Evobus) at the premises of the University Medicine Greifswald as part of the mobile preventive healthcare project PAKt-MV. It will be referred to as the mobile Preventiometer. The second Preventiometer was installed in an office within the Department of General Practice. It will be referred to as the stationary Preventiometer. Five examinations of the Preventiometer were comparable to examinations of SHIP (see Study 2): Somatometry, blood pressure measurement, body fat measurement, pulse oximetry and spirometry (see Table 1 for a detailed overview). Because somatometric examinations were conducted outside the Preventiometer device, they were only assessed once and are therefore not subject to reliability analysis.

Examinations within the Preventiometer were conducted by study nurses who were first trained in the SHIP examination center for basic examinations (somatometry, blood pressure measurement, and spirometry) and then trained by instructors from the manufacturer of the Preventiometer.

Page 3 of 18

Design

Study 1 followed a repeated measurement design, i.e. each participant was examined twice in a Preventiometer in immediate succession. The examinations within Preventiometers were always conducted in the following order: Somatometry (only at the first measurement occasion), blood pressure and body fat measurement, pulse oximetry and spirometry. A subset of the participants (n=22 with a mean age of 32.7 [SD=8.65], consisting of 7 males and 15 females) were examined *twice* in *each* Preventiometer in immediate succession, thus contributing data for the analysis of both Preventiometers (in contrast to participants that were tested *twice* in *one* of the Preventiometer are described in detail below.

Somatometry Height was measured using a stadiometer. Participants were asked to remove their shoes for this measurement. For the waist and hip circumferences a simple measuring tape was used. For the weighting participants stripped down to their underwear.

Blood pressure and body fat measurement Systolic and diastolic blood pressure and body fat percentage were both measured with the OEM version of the Health-Guard-15 Portable Health Kiosk. It consists of an oscillometric blood pressure measurement device and a near-infrared interactance body fat measurement device [13]. The cuff for the blood pressure measurement was applied to the left and the body fat sensor to the triceps of the right arm of the participant. Both measurements were taken simultaneously. This measurement was taken after non-exhausting activities (i.e., somatometry), but no specified resting phase was implemented. This procedure followed the suggestions by the manufacturer.

Examination	Variable	Preventiometer	SHIP
Somatometry	Body height	Seca 213 stadiometer	Body length measuring device SOEHNLE
	Body weight	A&D UC-321PL	SOEHNLE S20
	Waist circumference	Seca 201 tape	Schneider tape
	Hip circumference		
Blood pressure measurement	Systolic blood pressure	HealthGuard-15 Portable Health	Omron 705 IT
	Diastolic blood pressure	Kiosk OEM	
Body fat measurement	Body fat (%)	Futrex PM 860	Bod Pod (Cosmed)
Pulse measurement	Heart rate	Nonin 3231 USB	Omron 705 IT
Spirometry	Peak Flow (PEF)	Carefusion SpiroUSB	Viasys Healthcare Masterscreen
	Vital capacity (FVC)		

Table 1 Comparable examinations and the corresponding measurement instruments of the Preventiometer and SHIP

Pulse oximetry For pulse oximetry, a Nonin 3231 USB Pulse oximeter was used that was attached to the right index finger of the participant.

Spirometry Spirometric parameters were measured with the Carefusion SpiroUSB spirometer. At least three expiratory maneuvers were conducted from which the best trial was selected to determine the spirometric parameters of interest. The procedure followed a detailed SOP that was in line with German guidelines [14] as far as the expiratory part of spirometry is concerned.

Statistical analysis

We evaluated the reliability of measurements by means of intra-class correlation coefficients (ICC) as a two-way random effects model with absolute agreement and single measurement [15]. We considered ICCs \geq 0.70 as indicative of acceptable reliability [16]. Additionally, we report the variance components (VC) for persons, replications and residuals estimated by the ICC function from the R package *psych* to allow for a differentiation of systematic and random measurement error and the standard error of measurement for agreement (SEM_{agreement}) as proposed by Vet et al. [17]. Furthermore, we computed the mean of differences (i.e. bias) between repeated measurements within participants, the standardized mean difference (SMD), and the limits of agreement (LoA) for the repeated measurements. The SMD was computed as the mean of the differences (i.e. bias) between repeated measurements within participants divided by the standard deviation of these differences, and the limits of agreement were computed as the mean of the differences (i.e. bias) ± 1.96 times the standard deviation of the differences between the first and second measurements.

Finally, we plotted the differences against the averages according to Bland and Altman [18] to allow for a visual inspection of (dis-)agreement between the measurements. All analyses were conducted separately for the mobile and the stationary Preventiometer.

All data were complete. All calculations were performed with the statistical software R [19] and additional R packages [20–25].

Results

All examinations have ICCs above 0.70 (see Table 2). ICCs for diastolic blood pressure (mobile), body fat, heart rate (mobile) and spirometric variables surpass 0.90. There are no substantial *mean differences* between the first and second measurement in the Bland–Altmanplots (see Fig. 2 and Fig. 3). However, observed extreme differences between observations primarily concerned the mobile Preventiometer. This is also in line with the

tendency of the variance component of the replications to be higher for the mobile Preventiometer in the case of blood pressure and heart rate measurements.

Discussion

In both Preventiometers, retest-reliability estimates were excellent for *body fat, vital capacity,* and *peak flow* whereas agreement for the *systolic blood pressure, dias-tolic blood pressure* and *heart rate* was lower but still in the acceptable range [16].

To put our result in context, we compared them with results from other reliability studies (Table 3). Overall, reliability in terms of ICCs are mostly in line with comparable method comparison studies and can be regarded as sufficient, yet some discrepancies are noteworthy. For example, in the context of the HERITAGE family study [26], ICCs for blood pressure were somewhat smaller than in our study. This may be explained by the larger time interval between measurements in the HERITAGE study (one day vs. approximately one hour). The ICCs from a study evaluating the reliability of a predecessor of the body fat measurement device built into the Preventiometer [27] were slightly smaller than in our study. ICCs for heart rate measurements in our study lie in the middle of the range of ICCs that have been reported in two studies comparing different devices for the measurement of heart rate [4, 28]. Whereas the ICCs for Peak flow (PEF) are in line with observed ICCs from other studies [29, 30], ICCs for FVC in our study are larger. This may be due to the shorter time interval between both measurements. Overall, the mean differences between the first and second measurements were small. Foremost in the mobile Preventiometer, heart rate seems to decrease slightly between the first and second measurement. This may reflect an adaptation to the new and mildly exciting examination context in the mobile Preventiometer.

Study 2: agreement between Preventiometer and SHIP measurements (validity)

The aim of Study 2 was to estimate the measurement agreement of Preventiometer examinations with comparable examinations in a population-based cohort study, the Study of Health in Pomerania (SHIP). This provides insights into the usability of Preventiometer measurements instead of SHIP measurements, for example when potential participants can better be accessed by allowing for a mobile assessment close to their homes. SHIP comprises two cohorts, and a large range of health related variables have been assessed. More details have been described elsewhere [10–12]. SHIP is subject to rigorous internal and external quality control Therefore, data from SHIP was used as reference for the Preventiometer.

)			_									
Variable	۶	1 st Meas M (SD)	2 nd Meas M (SD)	Mean difference [Cl]	SMD	Lower LoA [CI]	Upper LoA [CI]	2 []]	VC persons	VC methods	VC residuals	SEM agreement
Systolic blood p	oressure	e in mmHg										
Mobile	45	120.5 (13.8)	122.1 (13.8)	1.6 [-0.2; 3.5]	0.27	-13.8 [-17; -10.6]	10.5 [7.3; 13.7]	.90 [.82; .94]	171.96	0.93	19.21	4.49
Stationary	31	122.5 (12.9)	121.9 (13.2)	-0.6 [-2.8; 1.6]	-0.1	-11.3 [-15.1; -7.5]	12.5 [8.6; 16.3]	.89 [.79; .95]	152.14	0	17.94	4.24
Diastolic blood	pressu	re in mmHg										
Mobile	45	79.5 (9.4)	81.1 (9.6)	1.6 [0.5; 2.8]	0.42	-9.2 [-11.2; -7.2]	6 [4; 8]	.91 [.82; .95]	82.68	1.15	7.48	2.94
Stationary	31	79.1 (8.8)	80.7 (9.6)	-1.6 [-0.2; 3.5]	0.32	-11.5 [-14.7; -8.3]	8.3 [5.1; 11.5]	.84 [.69; .92]	71.96	0.89	12.82	3.70
Body fat in %												
Mobile	45	29.6 (8.7)	30 (8.6)	0.4 [-0.3; 1.1]	0.19	-4.8 [-6; -3.6]	4 [2.8; 5.1]	.97 [.94; .98]	71.78	0.03	2.51	1.59
Stationary	31	28.3 (9.5)	29.1 (9.5)	0.7 [-0.1; 1.5]	0.34	-4.8 [-6.2; -3.5]	3.4 [2.1; 4.7]	.97 [.94; .99]	87.69	0.19	2.21	1.55
Heart rate in bg	шc											
Mobile	4	70.2 (11.9)	67.6 (10.9)	-2.6 [-4; -1.2]	-0.58	-6.3 [-8.7; -3.9]	11.6 [9.2; 14]	.90 [.75; .95]	120.33	3.24	10.40	3.69
Stationary	30	74.2 (10.6)	73.1 (10)	-1 [-2.8; 0.8]	-0.21	-8.4 [-11.5; -5.3]	10.5 [7.4; 13.6]	.89 [.78; .95]	94.77	0.15	11.60	3.43
Vital capacity (f	-VC) in I	_										
Mobile	46	4.3 (1.1)	4.3 (1.1)	0 [0; 0]	-0.01	-0.2 [-0.3; -0.2]	0.2 [0.2; 0.3]	.99 [1;99; 1]	1.20	0	0.01	0.08
Stationary	29	4.5 (1.2)	4.5 (1.2)	0 [-0.1; 0]	-0.16	-0.2 [-0.3; -0.1]	0.3 [0.2; 0.3]	1 [.99; 1]	1.44	0	0.01	0.08
Peak flow (PEF)	i.											
Mobile	46	7.8 (2.1)	7.8 (2.3)	0 [-0.1; 0.2]	0.08	-1.2 [-1.5; -0.9]	1.1 [0.8; 1.4]	.97 [.94; .98]	4.63	0	0.17	0.41
Stationary	29	7.8 (2)	7.7 (1.9)	-0.1 [-0.3; 0.1]	-0.24	-0.9 [-1.2; -0.5]	1.1 [0.8; 1.4]	.97 [.93; .98]	3.79	0	0.12	0.36
Meas. Measurem	ient, M n	nean, SD stands	ard deviation, Cl	confidence interval, LoA limit	of agreen	ient, ICC intraclass corr	relation coefficient, VC	variance com	ponents, SEM	standard error o	f measurement	

 Table 2
 Agreement between repeated measurements for mobile and stationary Preventiometers



Fig. 2 Bland–Altman Plots for repeated measurements within Preventiometer 1 (mobile)

Materials and methods *Study sample*

Study sumple

In total, 155 (53% female) participants of the SHIP-Trend-1 cohort [11] with a mean age of 57 years (SD=13) were enrolled. Recruitment for additional Preventiometer assessments took place at the SHIP examination center after participants completed their SHIP examinations on the same day. All participants gave written informed consent. The Ethics Committee of the University Medicine Greifswald approved the study protocol.

Design

The design of Study 2 followed a method comparison study design with a single measurement on each



Fig. 3 Bland–Altman Plots for repeated measurements within Preventiometer 2 (stationary)

method [32]. Participants were first examined in the SHIP study center and afterwards in one of the two Preventiometers. The time interval between the two measurements was about 1 to 6 h. Examinations in SHIP were conducted by certified SHIP examiners whereas examinations in the Preventiometers were performed by examiners of the project PAKt-MV who

were trained both in the SHIP study center and on the Preventiometer.

Examinations

Examinations of the Preventiometer have been described in the methods section of Study 1. Detailed descriptions of SHIP examinations can be found elsewhere (e.g., blood pressure, height, weight, and waist circumference [33];

Study	Devices	Comparison	Variable	n	ICC
Burkard et al. 2018 [31]	Omron HBP-1300	First vs. mean of second to fourth measurement	Systolic BP	802	.85
			Diastolic BP	802	.87
Stanforth et al. 2000 [26]	Colin STBP-780	Means of measurements (4 – 8) between two consecutive days	Systolic BP	822	.84
			Diastolic BP	822	.79
Nielsen et al. 1992 [27]	Futrex-5000	within-day	% body fat	34	.91
		between-day	% body fat	34	.95
Mitchell et al. 2016 [4]	Android app	Test-retest with 5 min interval	Heart rate	111	.82
	iOS app		Heart rate	111	.76
	Polar watch		Heart rate	111	.84
Losa-Iglesias et al. 2016 [28]	Radial pulse	Test-retest with 3 consecutive measurements	Heart rate	46	.99
	Pulsoximeter		Heart rate	46	.99
	Арр		Heart rate	46	.97
Krug et al. 2011 [29]	not specified	Repeated measurement between 3 to 16 days apart	FVC	633	.87
Fonseca et al. 2005 [30]	PiKo-1	Within-session reliability of two best maneuvers	PEF	38	.96
	Spirotel		PEF	38	.97
	Mini-Wright		PEF	38	.95

Table 3 Reliability estimates from similar method comparison studies

spirometry [34, 35]). A comparison of the instruments is displayed in Table 1. In the following section, we focus on methodological differences between Preventiometer and SHIP that might be of relevance for the evaluation of their agreement.

Somatometry Whereas body height is measured with a mechanical stadiometer in the Preventiometer, it is measured via an ultrasound method in SHIP. Weight and waist circumference variables are measured using similar measurement techniques (see Table 1). Participants were asked to take off their shoes for height measurement and strip to their underwear for weight measurement.

Blood pressure measurement Blood pressure is measured in the Preventiometer and SHIP by automatic oscillometric devices. However, in the Preventiometer, blood pressure is measured once without an explicit resting phase before the measurement, while blood pressure is measured three times in SHIP and the final value is computed as the mean of the second and third measurement. Before the first measurement, there is a five-minute resting phase in SHIP and between the three measurements, there are three minutes pauses. Finally, in the Preventiometer, blood pressure is measured on the left arm whereas in the SHIP, blood pressure is measured on the right arm.

Body fat measurement Body fat percentage is measured by a near infrared interactance device in the Preventiometer where a sensor is placed on the triceps of the participant. On the basis of this measurement, the fat percentage of the whole body is extrapolated. In contrast, in SHIP body fat percentage is measured using a Bod Pod, which uses air displacement plethysmography [36–39].

Pulse oximetry Heart rate is measured by a pulse oximeter in the Preventiometer. In SHIP, heart rate is determined during the course of blood pressure measurement by the blood pressure device.

Spirometry The spirometry device in the Preventiometer only recorded expiratory maneuvers but did not allow measurements of inspiratory maneuvers while in SHIP, an inspiratory and an expiratory maneuver was conducted.

Statistical analysis

We evaluated the agreement between measurements analogous to Study 1. Again, all analyses were conducted separately for the mobile and the stationary Preventiometer.

We excluded five data pairs from the analyses. In two cases, body weight was measured fully clothed in the Preventiometer which violated the study protocol. In another two cases, extreme differences for body height measurement (128.2 cm in the Preventiometer vs. 168 cm in the SHIP and 159.5 cm in the Preventiometer vs 170 cm in the SHIP, respectively) were most likely due to data input errors in the Preventiometer. Finally, an extremely large difference for body weight measurement was detected (81.9 kg in the Preventiometer vs. 112.9 kg in the SHIP).

and SHIP measurements
stationary)
(mobile and
^p reventiometer
ement between F
Table 4 Agre

	=		SHIP	Bias [CI]	SMD	Lower LoA [CI]	Upper LoA [CI]	ICC [CI]	V V	٨C	٨C	SEM agreement
		M (SD)	M (SD)						persons	methods	residuals	
Body height in cr	F											
Mobile	44	171 (9.2)	1 70.8 (8.8)	-0.2 [-0.5; 0]	-0.25	-1.4 [-1.8; -1]	1.8 [1.4; 2.3]	1 [.99; 1]	80.83	0.01	0.34	0.59
Stationary	102	171.2 (9.4)	171.1 (9.1)	-0.1 [-0.3; 0.2]	-0.06	-2.1 [-2.5; -1.8]	2.3 [1.9; 2.7]	.99 [69. ;99]	85.29	0	0.64	0.80
Body weight in k	n											
Mobile	44	83.7 (16.1)	82.6 (16)	-1.1 [-1.4; -0.8]	-1.13	-0.8 [-1.4; -0.3]	3.1 [2.6; 3.6]	1 [.94; 1]	257.04	0.63	0.50	1.06
Stationary	101	85.6 (16)	85.2 (16.1)	-0.4 [-0.5; -0.2]	-0.56	-1 [-1.2; -0.7]	1.7 [1.5; 1.9]	1 [1; 1]	257.21	0.07	0.23	0.55
Waist circumferer	nce in cm	6										
Mobile	46	94.5 (13.9)	96.6 (13.2)	2.1 [0.9; 3.4]	0.5	-10.4 [-12.6; -8.3]	6.2 [4; 8.4]	.94 [.87; .97]	175.65	2.05	6	3.32
Stationary	100	97.7 (14.9)	99.1 (14.6)	1.4 [0.5; 2.3]	0.3	-10.5 [-12.1; -8.9]	7.7 [6.1; 9.2]	.95 [.92; .97]	207.55	0.89	10.73	3.41
Hip circumferenc	e in cm											
Mobile	46	101.4 (10.4)	101.8 (10.5)	0.4 [-1; 1.7]	0.08	-9.2 [-11.5; -6.9]	8.5 [6.2; 10.8]	.91 [.84; .95]	99.17	0	9.97	3.16
Stationary	100	103.3 (10.8)	103.7 (10.7)	0.4 [-0.3; 1.2]	0.11	-7.9 [-9.2; -6.6]	7 [5.7; 8.3]	.94 [.91; .96]	107.58	0.02	7.26	2.70
Systolic blood pre	essure in	mmHg										
Mobile	44	123.6 (14.7)	121.6 (13.1)	-2.1 [-4.8; 0.6]	-0.23	-15.4 [-20.1; -10.7]	19.6 [14.9; 24.2]	.79 [.65; .88]	153.44	1.23	39.79	6.41
Stationary	66	131.9 (17.7)	127.8 (16.9)	-4.2 [-6.8; -1.5]	-0.31	-21.9 [-26.5; -17.4]	30.3 [25.7; 34.8]	.69 [.55; .78]	211.07	7.78	88.68	9.82
Diastolic blood p	ressure ir	n mmHg										
Mobile	44	80.2 (11.1)	72.8 (8.5)	-7.4 [-9.9; -4.8]	-0.88	-9.1 [-13.5; -4.7]	23.9 [19.5; 28.3]	.50 [.04; .75]	62.75	26.47	35.36	7.86
Stationary	66	80.3 (8.9)	75.2 (9.6)	-5.2 [-6.6; -3.7]	-0.7	-9.3 [-11.8; -6.8]	19.6 [17.1; 22.1]	.59 [.25;.77]	58.09	13.02	27.19	6.34
Body fat in %												
Mobile	33	33.3 (7.8)	33.3 (9.4)	0 [-1 <i>.</i> 7; 1 <i>.</i> 7]	0	-9.5 [-12.4; -6.5]	9.5 [6.5; 12.4]	.85 [.71; .92]	62.59	0	11.31	3.36
Stationary	67	33.2 (8.6)	34.9 (10)	1.7 [0.6; 2.8]	0.3	-12.7 [-14.6; -10.8]	9.3 [7.4; 11.2]	.81 [.71; .87]	70.81	1.29	15.73	4.13
Heart rate in bpn	C											
Mobile	44	74.9 (11.4)	72.3 (11.6)	-2.6 [-4.9; -0.2]	-0.33	-12.6 [-16.7; -8.6]	17.8 [13.7; 21.8]	.76 [.59; .86]	101.75	2.61	30.10	5.72

Variable	<u>د</u>	Prev M (SD)	SHIP M (SD)	Bias [Cl]	SMD	Lower LoA [CI]	Upper LoA [CI]	ICC [CI]	VC persons	VC methods	VC residuals	SEM agreement
Stationary	66	70 (10.9)	70.1 (9.4)	0.2 [-1.4; 1.7]	0.02	-15.3 [-18; -12.7]	15 [12.4; 17.6]	.71 [.60; .80]	73.09	0	29.63	5.44
Vital capacity (F	VC) in l											
Mobile	37	4 (0.9)	4.2 (1)	0.2 [0.1; 0.3]	0.58	-0.9 [-1.1; -0.7]	0.5 [0.3; 0.7]	.92 [.80; .97]	0.90	0.02	0.06	0.27
Stationary	86	4 (1.1)	4.1 (1.2)	0.1 [0.1; 0.2]	0.51	-0.7 [-0.8; -0.6]	0.4 [0.3; 0.5]	.97 [.93; .98]	1.23	0.01	0.04	0.21
Peak flow (PEF)	ļ											
Mobile	37	7 (1.9)	7.2 (2.2)	0.2 [-0.2; 0.6]	0.17	-2.4 [-3.1; -1.8]	2 [1.4; 2.7]	.85 [.72; .92]	3.54	0	0.64	0.80
Stationary	86	7.4 (2.3)	7.5 (2.3)	0.1 [-0.2; 0.4]	60.0	-2.6 [-3; -2.1]	2.3 [1.9; 2.8]	.85 [.78; .90]	4.57	0	0.79	0.89
n number of par	icipants, F	rev. Preventio	meter, M mean, 5	D standard deviati	ion, Cl confi	dence interval, <i>SMD</i> sta	ındardized mean differ€	ance, LoA limit o	f agreement, <i>I</i> C	C intraclass corre	lation coefficient,	VC variance

Table 4 (continued)

ed mean difference, LoA limit of agreement, ICC intraclass correlation coefficient, VC variance	
reventiometer, <i>M</i> mean, <i>SD</i> standard deviation, <i>C</i> / confidence interval, <i>SMD</i> standardize	r of measurement
n number of participants, Prev. F	components, SEM standard errc

This was also attributed to a data input error in the Preventiometer. Additionally, there were a few missing comparisons per examination (see Table 4) which were due to occasional malfunctions of the Preventiometer and missing values in the SHIP. All calculations were performed with the statistical software R [19] and additional packages [20–25].

Results

All ICCs were larger than 0.70, except for *systolic blood pressure* in the stationary Preventiometer and *diastolic blood pressure* in both Preventiometers.

Positive bias (i.e., Preventiometer measurements larger than SHIP measurements on average) were found for *body height, body weight, systolic* and *diastolic blood pressure* and *heart rate* (mobile Preventiometer). Negative bias (i.e., Preventiometer measurements smaller than their SHIP counterparts on average) were found for *waist* and *hip circumference, vital capacity* and *peak flow* and *heart rate* (stationary Preventiometer).

Comparing the Bland-Altman Plots for hip and waist circumference for the mobile Preventiometer (Fig. 4), the size of the LoA for hip circumference measurements is mainly driven by some extremely large differences, even after the outlier elimination, whereas the range of the LoA for waist circumference measurements is based on a more consistent distribution of the differences. There is also evidence for proportional bias (i.e. a statistically significant slope in the regression of the differences on the averages) in the Bland–Altman plots of body height, diastolic blood pressure, body fat and vital capacity for the mobile Preventiometer. Regarding the stationary Preventiometer (Fig. 5), some extreme differences between measurements occurred that are located by a far margin outside the limits of agreement. In the cases of *hip* and waist circumference measurements, differences around 20 cm occurred. For systolic blood pressure measurement, there are two differences around or even above 50 mmHg. This is also reflected in a much higher variance component of methods for the stationary Preventiometer for these measurements. Furthermore, there is evidence for proportional bias (see above) for body *height, heart rate, body fat and vital capacity.*

Discussion

In Study 2, we assessed measurement agreement from a mobile and a stationary Preventiometer with measurements obtained during SHIP examinations. While SHIP measurements can be conceived as a proxy to validity, there are two concerns that limit this interpretation: (1) Some of the measures change over the course of the day, such as blood pressure. There were up to several hours between both measurements because participants were first fully examined in SHIP and afterwards in one of the Preventiometers. (2) Measurement protocols were not exactly the same.

Results from both Preventiometers were largely consistent. At least acceptable ICCs (>0.70) were found for all variables except for *blood pressure* measurements, where ICCs between 0.5 and 0.6 occurred. In both Preventiometers, blood pressure measurements were higher compared to their SHIP counterparts whereas the opposite was true for *spirometric measurements*.

Table 5 displays an overview of results from method comparison studies with similar variables. Four studies reported ICCs and/or bias and limits of agreement for *somatometric* variables. The observed mean differences in our study for *body height, body weight, hip,* and *waist* measurements are not larger in comparison but the limits of agreement for *hip* and *waist* measurements are. The latter indicates the presence of more unsystematic measurement error in the Preventiometer assessment.

Method comparison studies related to *blood pressure* measurement reported a wide range of agreement indices depending on the compared methods, the context of measurement, and the duration between measurements. Bias and limits of agreement we observed in our study lie at the upper end compared to these studies. The strict criterion proposed by the European Society of Hypertension according to which 95% limits of agreement should not exceed 15 mmHg was not met [57]. The observed differences may be explained by the procedural differences as outlined above, particularly the lack of a systematic resting period prior to the measurements due to the interest of shortening the examination time, and the time-interval between Preventiometer and SHIP measurements.

ICCs for *body fat* seemed relatively low when compared to other measures. A study comparing near-infrared interactance (NIA)-the same method as implemented in the Preventiometer-and dual-energy X-ray absorptiometry (DXA) body fat measurement reported absolute bias and limits of agreement that fall into the same range as the present study [44]. However, the same study reported smaller absolute bias values and narrower limits of agreement when comparing bioelectrical impedance analysis (BIA) to DXA. In another study comparing BIA and calipometry to hydrodensitometry, even smaller bias values and narrower limits of agreement are reported [45]. The ICCs reported in a validation study evaluating the agreement between a commercial bioelectric impedance scale and calipometry are much higher than in the present study. Thus, our results are comparable to other studies using NIA, but better results might be achieved by using alternative methods of body fat measurement (BIA or calipometry).



Fig. 4 Bland-Altman plots for the comparison between Preventiometer 1 (mobile) and SHIP measurements



Fig. 5 Bland-Altman plots for the comparison between Preventiometer 2 (stationary) and SHIP measurements

Table 5 Agreement and validity estimates from similar method comparison studies

Authors	Device(s)	Comparison	Variable	Subgroup	n	Bias	LoA ^a	ICC
Jaeschke et al. 2015 [40]	Vitus Smart XXL	Manual measurement vs.	height	Men	27	0.6	1.8	
		Bodyscanner (see device)	waist	Men	27	1.5	5	
			hip	Men	27	2.3	2.6	
			height	Women	32	1.2	2	
			waist	Women	32	4.7	6.6	
			hip	Women	32	3	3.6	
McEneaney & Lennie 2011		Self- vs. professional	waist	Written instructions	29	1.75	6.4	
[41]		measurement / Self-meas-	hip	Written	29	-0.35	7.2	
		urement: Written vs. video	waist	Video	28	0.95	8	
		Instructions	hip	Video	28	-0.75	6.65	
Dekkers et al. 2008 [42]		Self-reported vs. manual	height		1298	-0.7	3	.99
		measurement	weiaht		1298	1.4	3.8	1
			waist		1298	-1.1	7.9	.96
Ross & Wing 2016 [43]	BodyTrace smart scale, BWB-800	Home scale vs. clinical measurement	weight		58	1.1	1.6	
Jensky-Squires et al. 2008	BioSpace InBody 320 (BIA1).	BIA1 vs. DXA	body fat%	Men	254	-2	6.4	
[44]	Omron (BIA2), Bod-eComm	BIA2 vs. DXA	body fat%	Men	217	-1	8.4	
	(NIA), dual-energy X-ray	NIA vs. DXA	body fat%	Men	252	-1.8	9.4	
	absorptionetry (DXA)	BIA1 vs DXA	body fat%	Women	254	-36	66	
		BIA2 vs. DXA	body fat%	Women	217	-33	7.8	
		NIA vs. DXA	body fat%	Women	252	-4.8	10.5	
Williams & Bale 1998 [45]	Harpenden skinfold caliper	HYD vs BIA	body fat%	female	115	-1.2	49	
	(SKF), BIA 101 (BIA), Hydro-	HYD vs. SKE	body fat%	female	115	-14	4.4	
	static weighing (HYD)	HYD vs. BIA	body fat%	male	117	0.6	4	
		HYD vs. SKF	body fat%	male	117	0.0	37	
Cassidy & Jones 2001 [46]		right-left arm 1st vs. 2nd	Svet RP	marc	237	1 77	27	
		measurement	Diact RD		237	3 73	20.6	
Christofaro et al. 2000 [47]	Omron MY3 Plus vs. Morcury	ICC from first massurament	Svet RD		165	2.75	10.1	80
	Official winds a flus vs. Mercury	measurement were taken	Diact RP		165	0.8	10.1	.00
		simultaneously	Diast. Di		105	0.0	10.5	./ 1
Agarwal 2016 [48]	Omron HEM 907, Omron	Measurement under	Syst. BP		275	-12.7	33.4	
	HEMI 705 CP	tions	Diast. BP		275	-12	22.1	
Vera-Cara et al. 2011 [49]	Omron HEM-705-CP	mean of 3 auscultatory vs.	Syst. BP		1084	1.80	11.9	
		mean of 2 oscillometric measurements	Diast. BP		1084	-1.60	10.8	
Smith & Hofmeyr 2019 [50]	Contec CMS50D, Nihon Koh- den Life Scope MU-631 RK	Fingertip pulse oximeter vs. conventional bedside monitor	Heart rate		220	-0.43	5.2	
Mitchell et al. 2016 [4]	Polar watch, Android App,	Polar vs. android	Heart rate		111	-1.75	7.5	.95
	iPhone App	Polar vs. iphone	Heart rate		111	-1	5.9	.97
Losa-Iglesias et al. 2016 [28]	Radial pulse (RAD). Nonin	RAD vs. OXI	Heart rate		46	-0.21	2 95	99
(<u></u> ,	GO2 (OXI), Heart Rate Plus	RAD vs APP	Heart rate		46	312	5 1 2	95
	(APP)	OXI vs. APP	Heart rate		46	3.24	5 21	94
Liistro et al. 2006 [51]	Vmax 20C Morgan TI C	Datospir 70	FVC ^b		399	-0.07	0.54	
2115110 61 011 2000 [51]	Datospir 70, Microloop,	Microloon	FVC ^b		399	-0.03	0.44	
	Spirobank	Spirobank	FVC ^b		399	-0.04	0.52	
Gerbase et al. 2013 [52]	SM 2200 (SM) FasyOne	FO1 vs SM	FVC ^b		82	-0.13	0.31	
	handhelds (EO1-EO3)	EO2 vs. SM	FVC ^b		82	-0.02	03	
		FO3 vs. SM	FVC ^b		82	-0.02	03	
						0.07	0.0	

Page	15	of	18
------	----	----	----

Authors	Device(s)	Comparison	Variable	Subgroup	n	Bias	LoA ^a	ICC
Wiltshire & Kendrick 1994	Escort spirometer, Model S	Escort vs. Wedge	FVC ^b		113	0.03	0.56	
[53]	wedge bellows spirometer, Wright peak flow meter	Escort vs. Wright	PEF		113	0.03	1.7	
Swart et al. 2003 [54]	Spirospec desktop spirom-		FVC ^b		45	0.03	0.24	
	eter, Masterlab 4.0 standard spirometer		PEF		45	-0.41	1.12	
Rebuck et al. 1996 [55]	Welch-Allyn Pneumocheck,		FVC ^b		75	0.06	0.56	
	P.K. Morgan Sprioflow 12		PEF		75	0.44	1.9	
Maree et al. 2001 [56]	Diagnosa, Masterlab 4.0		FVC ^b		45	-0.1	0.22	
			PEF		45	-0.03	1.18	
Fonseca et al. 2005 [30]	PiKo-1, Spirotel, Mini-	PiKo-1 vs. reference	PEF		38	0.22	1.48	.90
	Wright, Vitalograph 2120	Spirotel vs. reference	PEF		38	-0.35	1.53	.95
	(rererence)	Mini-Wright vs. reference	PEF		38	-1.15	2.9	.87

n number of participants, LoA limit of agreement, ICC intraclass correlation coefficient

^a Because detailed information about limits of agreement often lacks, we report the crude LoA, computed as the twofold standard deviation of the differences, here ^b We only include the comparisons of spirometers with a turbine as flow sensor (as in our studies) to the standard spirometers

Bias for *heart rate* measurement is comparable to other studies, yet, limits of agreement in our study are much larger while ICCs are lower. This might be due to the comparatively large time-interval between the Preventiometer and SHIP measurements and the lack of a resting phase before measurements in the Preventiometer.

Regarding spirometric measurements, estimates of bias and limits of agreement found in Study 2 were at the upper end of the range of what has been found in similar studies. One study also reports ICCs for *peak flow* measurements that are slightly higher than ICCs obtained in our study [24].

General discussion

Overall, while Preventiometer examinations have adequate reliability according to conventional cut-offs [16], which are in line with results from comparable methods studies (Table 3): Yet, there are some issues to be overcome to increase the comparability of results to the conventional assessment of the studied biomarkers in a cohort study. Measurement agreement was acceptable for most examinations with the exception of *blood pressure*. The consistently higher blood pressure measurements in the Preventiometer may be dealt with by introducing a larger resting period before, and by repeating measurements. In addition, the limits of agreement for most examinations were large compared to other method comparison studies dealing with similar variables. This likely reflects a relevant influence of random measurement error which is also supported by the fact that variance components of methods were consistently smaller than variance components of residuals in the ICC models, respectively. However, one has also to take into account the natural clinical outcome: For example, systolic blood pressure, diastolic blood pressure, and pulse rate can be expected to have lower agreement than body fat or body weight because the underlying physiological magnitudes and processes are more volatile [58]. Thus, the comparatively low ICCs and large limits of agreement for *blood pressure* and *heart rate* may be partly explained by this variability. Another source of disagreement is probably rooted in the methodological and procedural differences described in the discussions of Study 1 and Study 2 (e.g., resting phases, time-intervals). Therefore, a better agreement between *blood pressure* measurements in Preventiometer and SHIP may be expected, if the procedures were harmonized.

In contrast to *blood pressure* and *heart rate*, natural variability may not explain discrepancies with regards to *body fat* measurements. The body fat measurement device in the Preventiometer only measures body fat values up to 45% whereas the Bod Pod (SHIP) does not have this technical measurement limit. Inspecting the Bland–Altman Plots for the comparisons of body fat measurement, this problem becomes visible in form of the points lying on the decreasing line at the right end of the plot. However, we decided to not exclude these data points since this problem may arise in many application contexts with normal populations (which also include people with body fat percentages above 45%) and thus, this technical measurement limit also impairs the validity.

To improve the comparability of the Preventiometer results, we suggest the following steps: (1) *Blood pressure* measurement should follow procedures of available guidelines [59], that is at least two successive measurements shall be obtained and a resting pause of 5 min

should be implemented before the first measurement. (2) Spirometry should be extended by the inspiratory part of the examination as recommended in relevant guidelines. This has been already implemented in the course of PAKt-MV. (3) The body fat measurement device should be replaced by a more valid device. The actual near-infrared interactance body fat device not only has considerable disagreement with the Bod Pod device from SHIP but it also has a technical measurement limit at 45% (see above). While near-infrared interactance is a very timeefficient measurement method to assess body fat, one should keep in mind that it is usually applied to one body point only, while the more valid and traditional skinfold method is applied to multiple body points and an algorithm is used to compute overall body fat [60]. Therefore - technical limitations notwithstanding, multiple body points might be measured with the near-infrared interactance method, thereby combining the time-efficiency of the near-infrared interactance method with the validity of the skinfold method. However, testing the validity using multiple vs. single measuring points with the nearinfrared interactance method, Heyward et al. [61] found only a small advantage using multiple measuring points.

Limitations

Repeated measurements within a single study would have allowed for a variance decomposition and better estimation of the measurement error (a) due to the Preventiometer, (b) due to SHIP, and (c) due to the lack of agreement between Preventiometer and SHIP. However, logistical constraints required that SHIP participants could only be examined once, allowing for no variation of the sequential order of Preventiometer and SHIP examinations in Study 2, and the Preventiometer examinations always took place after the SHIP examinations. We did not cover all potential measurements of the Preventiometer [5, 6] because we focused on measurements comparable to SHIP. Measurement properties are of relevance to provide an informed overview on the usefulness of the Preventiometer for participants and researchers alike. Yet, other aspects beyond the scope of this paper are of relevance as well. The positive user experience [7, 8] has been commented upon. We were also able to perform assessments right at the work place of participants, resulting in little to no travel time for them. Effects on response would need to be dealt with in a separate study. Another aspect is a formal comparison of staffing requirements. When using a bus, there must be a driver with an appropriate license. Overall, compared to stationary examinations, there may be little options to save personnel. On the other hand a very important issue is resolved. All data is collected electronically and stored in a single database. Therefore, background IT-infrastructure is provided, which is important from a provider perspective. In addition, a larger follow-up study is recommended, once the issues raised here have been resolved.

Conclusion

The initial motivation of these studies was to evaluate the Preventiometer for the use in a preventive health care project (PAKt-MV). As previously stated, reliability is a prerequisite for the detection of change within subjects over time. In our current evaluation, we found the Preventiometer's measurements sufficient in this regard. However, measurement agreement was insufficient for some measurements. While issues like the body fat measurements can be easily remedied by replacing the measurement device, the deviant blood pressure and pulse measures are an indication for a procedural issue. One of the reasons to use the Preventiometer is to save examination time, which benefits the examiners and the participants. To forgo the recommended resting periods for measuring blood pressure and pulse rate can be seen as a trade-off exchanging validity for time. Our findings suggest that insufficient resting periods have a strong biasing impact making a rather conservative point of trade-off to be preferable. Overall, methodological and technological improvements should be realized before using the Preventiometer in population-based research.

Abbreviations

BIA	Bioelectrical impedance analysis
DXA	Dual-energy X-ray absorptiometry
FVC	Vital capacity
HYD	Hydrostatic weighing
ICC	Interclass correlations coefficient
IMS	lpex management software
LoA	Limit of agreement
NIA	Near-infrared interactance
PAKt-MV	Prävention für Arbeitnehmer zur Reduktion von Krankheitstagen durch Motivation und Verbaltensänderung Ipreventive healtbcare
	for workers with the aim to reduce absenteeism by motivation
	and behavior]
PEF	Peak flow
PROMs	patient-reported outcome measures
RAD	Radial pulse
SEM	Standard error of measurement
SHIP	Study of Health in Pomerania
SKF	skinfold caliper
SMD	standardized mean difference
VC	Variance components

Supplementary Information

The online version contains supplementary material available at https://doi.org/10.1186/s12874-023-01911-x.

Additional file 1.

Acknowledgements

We wish to thank our study nurses Doris Jaeschke, Wieland Köhn, and Elisa Michalowski for their assistance.

Authors' contributions

The first draft was written by MK and MJ and further edited based on comments from all authors. The study was conceived and Funding was obtained by RB and COS. Data was analyzed by MJ, MK & COS. DW-R, BB, JFC, MB, and MD provided consulting on clinical measurements and were involved in the execution of the study. All authors approved the final version of the draft.

Funding

Open Access funding enabled and organized by Projekt DEAL. All results were obtained as part of the project PAKt-MV (supported by the European Regional Development Fund and the Ministerium für Wirtschaft, Bau und Tourismus: GW-16–0003 and GW-16–8008) in which Vilua and the University of Greifswald cooperated on a mobile health prevention project. SHIP is part of the Community Medicine Research Network of the University Medicine Greifswald, which is supported by the German Federal State of Mecklenburg-Western Pomerania. Bod Pod was funded by German Centre of Cardiovascular Research (DZHK)/BMBF (81X1400103).

Availability of data and materials

Data of the SHIP studies and associated projects are available upon reasonable request from the Transferstelle für Daten- und Biomaterialienmanagement [Office for transfer of data and bio materials] and can be applied for under: https://transfer.ship-med.uni-greifswald.de/FAIRequest/data-use-intro

Declarations

Ethics approval and consent to participate

All participants gave written informed consent. The Ethics Committee of the University Medicine Greifswald approved the study protocol (BB 100/17). The study was conducted in accordance with the institutional guidelines and all relevant national and international regulations.

Consent for publication

NA.

Competing interests

Markus Krüger was employed based on a cooperation project between the University Medicine Greifswald and Vilua. Reiner Biffar was a member of the corporate board of Vilua. The funders had no role in study design, data collection and analysis, decision to publish, or preparation of the manuscript. None of the other authors have any conflict of interest to declare.

Author details

¹Institute for Community Medicine, University of Greifswald, Greifswald, Germany. ²Present Address: nxt statista GmbH & Co. KG, Hamburg, Germany. ³Present Address: Unit of Prosthodontics, Gerodontology, and Biomaterials, Centre of Oral Health, University of Greifswald, Greifswald, Germany. ⁴Division of General Internal Medicine, Mayo Clinic, Rochester, MN, USA. ⁵Department of Internal Medicine B (Cardiology), University Medicine, Greifswald, Germany. ⁶German Centre for Cardiovascular Research (DZHK), Partner Site Greifswald, University of Greifswald, Greifswald, Germany. ⁷Department of General Practice, Institute for Community Medicine, University of Greifswald, Greifswald, Germany. ⁸Unit of Prosthodontics, Gerodontology, and Biomaterials, Centre of Oral Health, University of Greifswald, Greifswald, Germany.

Received: 18 February 2022 Accepted: 3 April 2023 Published online: 24 April 2023

References

 Galea S, Tracy M. Participation rates in epidemiologic studies. Ann Epidemiol. 2007;17(9):643–53. https://doi.org/10.1016/j.annepidem.2007.03. 013.

- Czajka JL, Beyler A. Background Paper Declining Response Rates in Federal Surveys: Trends and Implications. MATHEMATICA Policy Research, 2016.
- Hoffmann W, et al. Zum Problem der Response in epidemiologischen Studien in Deutschland (Teil II). Das Gesundheitswesen. 2004;66(08/09):482–91.
- Mitchell K, Graff M, Hedt C, Simmons J. Reliability and validity of a smartphone pulse rate application for the assessment of resting and elevated pulse rate. Physiother Theory Pract. 2016;32(6):494–9. https://doi.org/10. 1080/09593985.2016.1203046.
- "Preventiometer IPEXHealth." https://www.ipexhealth.com/en/product/ preventiometer/ (Accessed 10 May 2021).
- "CareCenter," Vilua. https://vilua.com/services/carecenter/ (Accessed 29 Apr 2021).
- Nanda S, et al. Evaluation of a Novel Wellness Assessment Device (Preventiometer): A Feasibility Pilot Study. Glob Adv Health Med. 2019;8:2164956119881096. https://doi.org/10.1177/2164956119881096.
- Nanda S, et al. Preventiometer, a Novel Wellness Assessment Device, Used With Healthy Volunteers: A Phase 2 Study. Glob Adv Health Med. 2021. https://doi.org/10.1177/21649561211045016.
- Universitätsmedizin Greifswald, "PAKt-MV," PAKt-MV mobile Gesundheitsförderung, https://www.pakt-mv.de/ (Accessed 12 Sep 2019).
- John U, et al. Study of Health in Pomerania (SHIP): a health examination survey in an East German region: objectives and design. Soz Präventivmed. 2001;46(3):186–94. https://doi.org/10.1007/BF01324255.
- Völzke H, et al. Cohort profile: the study of health in Pomerania. Int J Epidemiol. 2011;40(2):294–307. https://doi.org/10.1093/ije/dyp394.
- 12. "Forschungsverbund Community Medicine: SHIP." http://www2.medizin. uni-greifswald.de/cm/fv/ship/ (Accessed 14 Jun 2019).
- 13. Futrex, INC., "Health Guard Owner Manual PM 860."
- Criée C-P, et al. Leitlinie zur Spirometrie. Pneumologie. 2015;69(03):147– 64. https://doi.org/10.1055/s-0034-1391345.
- Shrout PE, Fleiss JL. Intraclass correlations: uses in assessing rater reliability. Psychol Bull. 1979;86(2):420–8. https://doi.org/10.1037/0033-2909. 86.2.420.
- Koo TK, Li MY. A guideline of selecting and reporting intraclass correlation coefficients for reliability research. J Chiropr Med. 2016;15(2):155–63. https://doi.org/10.1016/j.jcm.2016.02.012.
- de Vet HCW, Terwee CB, Knol DL, Bouter LM. When to use agreement versus reliability measures. J Clin Epidemiol. 2006;59(10):1033–9. https:// doi.org/10.1016/j.jclinepi.2005.10.015.
- Bland JM, Altman DG. Statistical methods for assessing agreement between two methods of clinical measurement. Lancet. 1986;1(8476):307–10.
- R Core Team. R: A Language and Environment for Statistical Computing. Vienna, Austria: R Foundation for Statistical Computing; 2018. Available:https://www.R-project.org/.
- 20. Revelle W. psych: Procedures for Psychological, Psychometric, and Personality Research. Evanston, Illinois: Northwestern University; 2018. Available: https://CRAN.R-project.org/package=psych.
- Gamer M, Lemon J, Singh IFP <puspendra.pusp22@gmail.com>, irr: Various Coefficients of Interrater Reliability and Agreement. 2019. Available: https://CRAN.R-project.org/package=irr.
- Datta D. blandr: a Bland-Altman Method Comparison package for R. 2017. https://doi.org/10.5281/zenodo.824514.
- 23. Wickham H. Reshaping Data with the reshape Package. J Stat Softw. 2007;21(12):1–20.
- 24. M. S. with contributions from T. Nunes et al., epiR: Tools for the Analysis of Epidemiological Data. 2018. Available: https://CRAN.R-project.org/packa ge=epiR.
- Grolemund G, Wickham H. Dates and Times Made Easy with lubridate. J Stat Softw. 2011;40(1):1–25. https://doi.org/10.18637/jss.v040.i03.
- Stanforth PR, et al. Reproducibility of Resting Blood Pressure and Heart Rate Measurements: The HERITAGE Family Study. Ann Epidemiol. 2000;10(5):7.
- Nielsen DH, Cassady SL, Wacker LM, Wessels AK, Wheelock BJ, Oppliger RA. Validation of the Futrex-5000 Near-Infrared Spectrophotometer Analyzer for Assessment of Body Composition. J Orthop Sports Phys Ther. 1992;16(6):7.
- 28. Losa-Iglesias ME, Becerro-de-Bengoa-Vallejo R, Becerro-de-Bengoa-Losa KR. Reliability and concurrent validity of a peripheral pulse oximeter and

health–app system for the quantification of heart rate in healthy adults. Health Informatics J. 2016;22(2):151–9. https://doi.org/10.1177/14604 58214540909.

- Krug LM, et al. Forced vital capacity (FVC) as a reproducible measure of pulmonary function (PF) in chemotherapy-pretreated patients with malignant pleural mesothelioma (MPM). JCO. 2011;29(15_suppl):7028– 7028. https://doi.org/10.1200/jco.2011.29.15_suppl.7028.
- Fonseca JA, et al. Pulmonary function electronic monitoring devices. Chest. 2005;128(3):1258–65. https://doi.org/10.1378/chest.128.3.1258.
- Burkard T, Mayr M, Winterhalder C, Leonardi L, Eckstein J, Vischer AS. Reliability of single office blood pressure measurements. Heart. 2018;104(14):1173–9. https://doi.org/10.1136/heartjnl-2017-312523.
- 32. Carstensen B. Comparing clinical measurement methods: a practical guide. Hoboken, N.J.: Wiley; 2013.
- Dittmann K, et al. U-shaped association between central body fat and the urinary albumin-to-creatinine ratio and microalbuminuria. BMC Nephrol. 2013;14(1):87. https://doi.org/10.1186/1471-2369-14-87.
- Stubbe B, et al. The Influence of Type 1 Diabetes Mellitus on Pulmonary Function and Exercise Capacity – Results from the Study of Health in Pomerania (SHIP). Exp Clin Endocrinol Diabetes. 2017;125(1):64–9. https:// doi.org/10.1055/s-0042-112219.
- Ewert R, et al. Lung Health Data of the Study of Health in Pomerania - a Review of Samples, Methods and First Results. Pneumologie. 2017;71(1):17–35. https://doi.org/10.1055/s-0042-117461.
- Anderson D. Reliability of air displacement plethysmography. J Strength Cond Res. 2007;21(1):169–72.
- Fields DA, Goran MI, McCrory MA. Body-composition assessment via air-displacement plethysmography in adults and children: a review. Am J Clin Nutr. 2002;75(3):453–67. https://doi.org/10.1093/ajcn/75.3.453.
- Levenhagen DK, et al. A comparison of air displacement plethysmography with three other techniques to determine body fat in healthy adults. J Parenter Enter Nutr. 1999;23(5):293–9. https://doi.org/10.1177/01486 07199023005293.
- Wingfield HL, Smith-Ryan AE, Woessner MN, Melvin MN, Fultz SN, Graff RM. Body composition assessment in overweight women: validation of air displacement plethysmography. Clin Physiol Funct Imaging. 2014;34(1):72–6. https://doi.org/10.1111/cpf.12067.
- Jaeschke L, Steinbrecher A, Pischon T. Measurement of waist and hip circumference with a body surface scanner: feasibility, validity, reliability, and correlations with markers of the metabolic syndrome. PLoS One. 2015;10(3):e0119430. https://doi.org/10.1371/journal.pone.0119430.
- McEneaney DF, Lennie SC. Video instructions improve accuracy of selfmeasures of waist circumference compared with written instructions. Public Health Nutr. 2011;14(7):1192–9. https://doi.org/10.1017/S1368 980011000450.
- Dekkers JC, van Wier MF, Hendriksen IJM, Twisk JWR, van Mechelen W. Accuracy of self-reported body weight, height and waist circumference in a Dutch overweight working population. BMC Med Res Methodol. 2008;8:69. https://doi.org/10.1186/1471-2288-8-69.
- 43. Ross KM, Wing RR. Concordance of in-home 'smart' scale measurement with body weight measured in-person. Obes Sci Pract. 2016;2(2):224–8. https://doi.org/10.1002/osp4.41.
- Jensky-Squires NE, Dieli-Conwright CM, Rossuello AE, Erceg DN, Mccauley SA, Schroeder ET. Validity and reliability of body composition analysers in children and adults. Br J Nutr. 2008;100(4):859–65. https://doi.org/10. 1017/s0007114508925460.
- Williams CA, Bale P. Bias and limits of agreement between hydrodensitometry, bioelectrical impedance and skinfold calipers measures of percentage body fat. Eur J Appl Physiol. 1998;77(3):271–7. https://doi.org/ 10.1007/s004210050332.
- Cassidy P, Jones K. A study of inter-arm blood pressure differences in primary care. J Hum Hypertens. 2001;15(8):519–22. https://doi.org/10. 1038/sj.jhh.1001224.
- Christofaro DGD, et al. Evaluation of the Omron MX3 Plus monitor for blood pressure measurement in adolescents. Eur J Pediatr. 2009;168(11):1349–54. https://doi.org/10.1007/s00431-009-0936-x.
- Agarwal R. Implications of Blood Pressure Measurement Technique for Implementation of Systolic Blood Pressure Intervention Trial (SPRINT). J Am Heart Assoc 2017;6(2). https://doi.org/10.1161/JAHA.116.004536.
- Vera-Cala LM, Orostegui M, Valencia-Angel LI, López N, Bautista LE. Accuracy of the Omron HEM-705 CP for blood pressure measurement in large

epidemiologic studies. Arq Bras Cardiol. 2011;96(5):393–8. https://doi.org/ 10.1590/s0066-782x2011005000038.

- Smith RN, Hofmeyr R. Perioperative comparison of the agreement between a portable fingertip pulse oximeter v. a conventional bedside pulse oximeter in adult patients (COMFORT trial). S Afr Med J. 2019;109(3):154–8. https://doi.org/10.7196/SAMJ.2019.v109i3.13633.
- Liistro G, Vanwelde C, Vincken W, Vandevoorde J, Verleden G, Buffels J. Technical and Functional Assessment of 10 Office Spirometers. Chest. 2006;130(3):657–65. https://doi.org/10.1378/chest.130.3.657.
- 52. Gerbase MW, et al. Agreement between spirometers: a challenge in the follow-up of patients and populations? Respiration. 2013;85(6):505–14. https://doi.org/10.1159/000346649.
- Wiltshire N, Kendrick AH. Evaluation of a new electronic spirometer: the vitalograph 'Escort' spirometer. Thorax. 1994;49(2):175–8. https://doi.org/ 10.1136/thx.49.2.175.
- Swart F, Schuurmans MM, Heydenreich JC, Pieper CH, Bolliger CT. Comparison of a new desktop spirometer (Spirospec) with a laboratory spirometer in a respiratory out-patient clinic. Respir Care. 2003;48(6):591–5.
- Rebuck DA, Hanania NA, D'Urzo AD, Chapman KR. The accuracy of a handheld portable spirometer. Chest. 1996;109(1):152–7. https://doi.org/ 10.1378/chest.109.1.152.
- Maree DM, Videler EA, Hallauer M, Pieper CH, Bolliger CT. Comparison of a New Desktop Spirometer (Diagnosa[®]) with a Laboratory Spirometer. RES. 2001;68(4):400–4. https://doi.org/10.1159/000050534.
- O'Brien E, Waeber B, Parati G, Staessen J, Myers MG. Blood pressure measuring devices: recommendations of the European Society of Hypertension. BMJ. 2001;322(7285):531–6.
- Parati G, Stergiou GS, Dolan E, Bilo G. Blood pressure variability: clinical relevance and application. J Clin Hypertens. 2018;20(7):1133–7. https:// doi.org/10.1111/jch.13304.
- Whelton PK, et al. 2017 ACC/AHA/AAPA/ABC/ACPM/AGS/APhA/ASH/ ASPC/NMA/PCNA Guideline for the Prevention, Detection, Evaluation, and Management of High Blood Pressure in Adults: A Report of the American College of Cardiology/American Heart Association Task Force on Clinical Practice Guidelines. Hypertension. 2018;71(6):e13–115. https:// doi.org/10.1161/HYP.00000000000065.
- Martín Moreno V, Gómez Gandoy B, Antoranz González MJ, Fernández Herranz S, Gómez de la Cámara A, de Oya Otero M. Validación del monitor de medición de la grasa corporal por impedancia bioeléctrica OMRON BF 300. Aten Primaria. 2001;28(3):174–81. https://doi.org/10. 1016/S0212-6567(01)78927-5.
- Heyward VH, et al. Validity of single-site and multi-site models for estimating body composition of women using near-infrared interactance. Am J Hum Biol. 1992;4(5):579–93. https://doi.org/10.1002/ajhb.1310040504.

Publisher's Note

Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.

Ready to submit your research? Choose BMC and benefit from:

- fast, convenient online submission
- thorough peer review by experienced researchers in your field
- rapid publication on acceptance
- support for research data, including large and complex data types
- gold Open Access which fosters wider collaboration and increased citations
- maximum visibility for your research: over 100M website views per year

At BMC, research is always in progress.

Learn more biomedcentral.com/submissions

